Morphology of the femoral neck in Japanese persons: Analysis using CT data

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Introduction: The purpose of this study was to analyze proximal femoral morphology in Japanese persons using computed tomography (CT) data.

Materials and methods: Data from 19 normal hips (N group) and 19 dysplastic hips (DH group) in women who underwent total hip arthroplasty were randomly selected from a CT database. The femur 3D model created by computer software was imported to a computer-aided design software package to analyze the medullary morphology. Center edge angle (CE angle), Sharp angle, femoral head diameter (FHD), and the offset were measured. The femoral neck isthmus space (FNIS), which is the narrowest part of the femoral neck, at neck-shaft angles of 125°, 130°, and 135°, was also measured.

Results: In the N group, CE angle was 36.2°, Sharp angle was 39.8°, FHD was 42.6 mm, and offset was 39.5 mm. In the DH group, CE angle was 24.7°, Sharp angle was 46.1°, FHD was 45.2 mm, and offset was 33.6 mm. Each parameter was significantly different between the groups. FNIS was 21.8 mm, 22.1 mm, and 22.1 mm, respectively, in the N group and 21.7 mm, 21.6 mm, and 21.5 mm, respectively, in the DH group.

Discussion: This is the first report to clarify the medullary morphology of the proximal femur in Japanese women. Results show that there is sufficient space for currently available implant to fit in. This study also elucidated the morphologic characteristics of dysplastic hip, which will be useful information in developing hip prostheses and fixation devices suitable for Asian patients.

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Key words: Morphology, femoral neck, CT data, femoral neck isthmus space

Introduction

The incidence of proximal femur fractures is continuing to increase in Japan¹⁾⁻³⁾. An estimated 180,000 patients had hip fractures in 2010. The age-adjusted incidence of hip fractures in Western countries is reportedly decreasing⁴⁾⁻⁷⁾, although the percentage of comminuted proximal femur fracture is reported to be increasing⁸⁾. The reason for the declining incidence going into the 21st century, despite the aging of society and increase in the elderly population in all countries, is unknown.

Early surgical treatment is recommended for proximal femur fractures 9^{1-11} . Treatment with a combination of lag screw and plate or intramedullary nail are widely used^{12), 13)}. Several types of lag screws and insertion angles of plate and nail have been developed to provide better treatment outcomes. However, because Asians usually have a smaller body constitution, including smaller femoral neck geometric parameters than Caucasians¹⁴⁾, implants developed in Europe and North America may have geometrical discrepancies to Asian patients¹⁵⁾. In addition, the morphology of the femoral neck in dysplastic hips differs from that of normal hips in terms of more severe anteversion, an aspheric head, and decreased offset¹⁶⁾⁻¹⁸⁾. Because of these morphological characteristics, insertion of lag screws and additional screws with optimal placement may be difficult in dysplastic hips of

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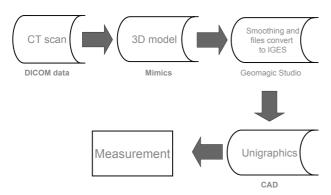
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Asian patients.

The purpose of this study was to analyze the femoral neck morphology of normal hips and dysplastic hips in Japanese women, and to evaluate the suitability of various implants used in Japanese patients.

Subjects and Methods

This study was approved by the Clinical Research Ethics Committee at Nagasaki University Hospital (approval number: 11082416). Data for 19 normal hips (N group) and 19 dysplastic hips (DH group) of Japanese women who underwent total hip arthroplasty were randomly selected from a digital imaging and communication in medicine (DICOM) computed tomography (CT) database using the "random" function of Microsoft Excel 2007 (Microsoft, Redmond, WA, USA). A dysplastic hip was defined by the criteria of the Nakamura et al.¹⁹⁾, a CE angle of 19° or less, a Sharp angle of 45° or less, and an acetabular roof angle of 15° or less, and they were measured by plain X-ray film. The DI-COM CT data were input into three-dimension (3D) model editing software (Mimics 9.0; Materialise Inc., Leuven, Belgium). Corticl bone and cancellous bone were segmented based on Hounsfield units (-37 to +1027 HU) described by Lamvohee et al.²⁰⁾, which were the appropriate threshold value. They were segmented for each CT slice, and a 3D model was created. Surface smoothing of the 3D model was achieved by using Geomagic Studio 7 (Geomagic Inc., Morrisville, NC, USA) and the files were converted to initial graphics exchange specification (IGES) files. Than 3D model was imported to computer-aided design (CAD) software (Unigraphics NX2; UGS PLM Software, Plano, TX, USA) (Figure 1).



As preparation before measurements, the method described by Noble et al.²¹⁾ was used to determine the position of the femoral head center. Approximate circles on femoral head slices were created from three arbitrary CT cross-sections of the femoral head on Mimics, and an approximate sphere of the femoral head was created from the three approximate circles to determine the position of the femoral head center (Figure 2a). The method of Noble et al.²¹⁾ was also used to determine the femoral axis. More specifically, the femoral axis was defined as a line connecting the center of cross-sections at distances of 50 mm and 80 mm from the lesser trochanter (Figure 2b). The position of the lesser trochanter was the tip in the 3D model. Cross-sections including the femoral axis and femoral head center were created (Figure 2c).

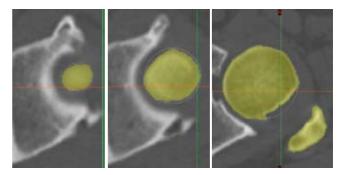




Figure 2a. An approximate sphere is created from three arbitrary cross-sections of the femoral head, and the center is defined as the femoral head center.

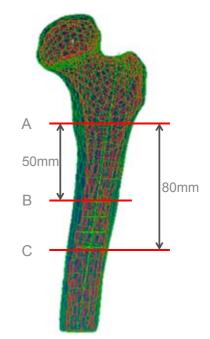


Figure 1. Flow chart of measurements

The acquired CT DICOM data were input into Mimics to create a 3D model, surface smoothing was performed using Geomagic Studio, and this was input into Unigraphics CAD software for measurements.

Figure 2b. The tip of the lesser trochanter (A) is identified on the 3D model. The femoral axis is defined as a line connecting the center of cross-sections at distances of 50 mm (B) and 80 mm (C) from the lesser trochanter tip.

Lines at angles of 125°, 130°, and 135° from the femoral head center to the femoral axis were drawn on each crosssection (Figure 2d). Two circles (circle C and D) were drawn to approximate the inside of the inferior and the superior cortex of the femoral neck, and lines parallel to the line created in figure 2d were drawn at locations as tangent lines to the circle C and D. The distance between these two parallel lines was defined as the femoral neck isthmus space (FNIS) (Figure 2e). The angle formed by the line connecting the femoral axis and femoral head center was defined as the femoral

neck-shaft angle. Anteversion was the angle made with cross-section of figure 2d (the section include femoral head center and femoral axis) and line drawn between the medial and lateral epicondyle of distal femur as described by Murphy et al.²²⁾. Medial and lateral epicondyle was identified as the tip in the 3D model.

In addition, anterior and posterior sections that included the neck axis, making an angle of 130° with the femoral axis, including the femoral head center, were created. On these cross-sections which was a shape of cancellous bone, circles

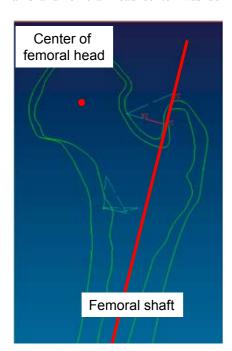


Figure 2c. A cross-section including the femoral axis and femoral head center is created.



Figure 2d. Lines at angles of 125° , 130° , and 135° from the femoral axis to the femoral head center are drawn.

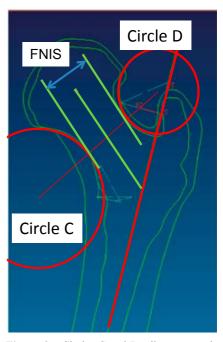


Figure 2e. Circles C and D adjacent superiorly and inferiorly to the femoral neck are created. Lines parallel to the line created in Fig. 3b are drawn at locations as tangent lines to the circles. The distance between these two parallel lines is defined as the FNIS.

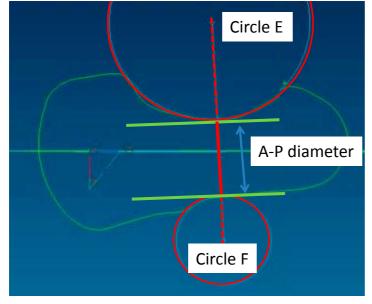


Figure 2f. For measurements on the lateral view, cross-sections including the femoral head center and making a 130° angle with the femoral axis are created. Circles E and F adjacent anteriorly and posteriorly to the femoral neck are created. Lines tangent to circles E and F and parallel to the line drawn from the femoral axis to the femoral head center are drawn. The distance between the two parallel lines is defined as the femoral neck A-P diameter.

E and F adjacent anteriorly and posteriorly to the femoral neck were created. The distance between the two tangent points with the femoral neck was defined as the femoral neck A-P diameter on the lateral view (Figure 2f). Moreover, femoral head diameter, version, neck shaft angle, offset of the femoral head center from the femoral axis, and femoral length were measured using CAD software. They were measured up to thrid decimal place and rounded to first decimal place. Statistical analysis was performed using the nonpaired t-test. Each data of FNIS and femoral neck A-P diameter on the lateral view was expressed as mean (minimummaximum).

Results

Mean age was 37.1 years in the N group and 38.7 years in the DH group. The mean CE angle was $36.2 \pm 6.5^{\circ}$ in the N group and $24.7 \pm 16.8^{\circ}$ in the DH group (p<0.05), and the

Table 1. Mean values of measured parameters

mean Sharp angle was $39.8 \pm 4.4^{\circ}$ in the N group and $46.1 \pm 3.0^{\circ}$ in the DH group (p<0.01). The mean femoral head diameter was 42.6 ± 3.6 mm in the N group and 45.2 ± 4.1 mm in the DH group (p<0.05). The mean anteversion angle was $32.1 \pm 9.5^{\circ}$ in the N group and $36.4 \pm 11.4^{\circ}$ in the DH group (p=0.21). The mean femoral neck-shaft angle was $129.7 \pm 5.4^{\circ}$ in the N group and $132.3 \pm 8.9^{\circ}$ in the DH group (p = 0.249). The mean offset of the femoral head center from the femoral axis was 39.5 ± 4.0 mm in the N group and 33.6 ± 4.3 mm in the DH group (p <0.01) (Table 1).

The mean FNIS in the N group was 22.1 mm (18.9-25.8 mm) at an angle of 125°, 22.1 mm (18.8-26.2 mm) at an angle of 130°, and 21.8 mm (18.7-25.9 mm) at an angle of 135° (Figure 3a). The mean FNIS in the DH group was 21.7 mm (16.3-25.9 mm) at an angle of 125°, 21.6 mm (16.3-26.2 mm) at an angle of 130°, and 21.5 mm (15.7-26.4 mm) at an angle of 135° (Figure 3b). The femoral neck A-P diameter on the lateral view was 20.4 mm (14.5-27.3 mm) in the N group and 19.7 mm (13.0-24.0 mm) in the DH group (Figure 3c).

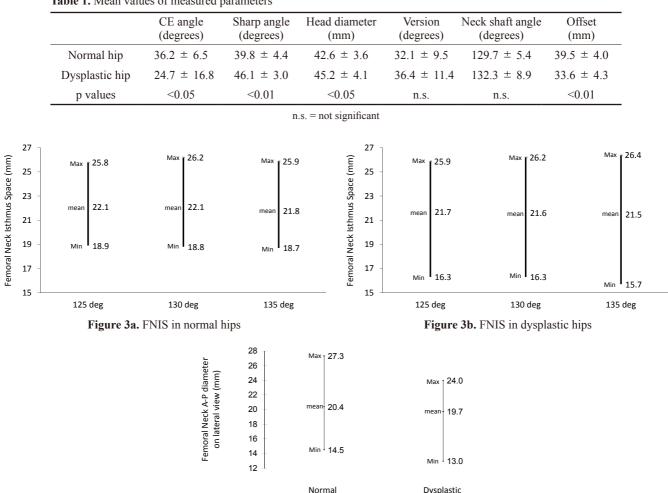


Figure 3c. Femoral neck A-P diameter on the lateral view

There were no significant differences in FNIS or femoral neck A-P diameter based on the presence or absence of hip dysplasia.

Discussion

Measurements of proximal femur morphology using CT have previously been reported^{17),18),23),24)} (Table 2). Argenson et al.¹⁸⁾ and Sugano et al.¹⁷⁾ compared hips with no or few morphological abnormalities and dysplastic hips, and as they reported, the present study also found more anteversion in dysplastic hips. However, the differences were not significantly different in our study. In addition, as reported by Argenson et al.¹⁸⁾, offset was significantly decreased in dysplastic hips compared to primary osteoarthritic hips. Although the measurement methodology differed in each study, the present results were similar to those of previous reports.

Early osteosynthesis is recommended for proximal femur fractures^{9),10)}. Treatment includes the use of sliding hip screws and short femoral nails¹²⁾. Baumgartner et al.²⁵⁾ reported that insertion of lag screws towards the femoral head center can decrease the rate of cut-out, the most common cause of postoperative failure. The diameter of implant lag screws currently used in Japan ranges from 10.3 mm to 15.3 mm (Table 3). The present study showed that these lag screws are suitable over an FNIS range and can be inserted

at ideal positions described by Baumgartner. It also showed that A-P diameter on the lateral view was large enough. However, the smallest FNIS values in the DH group were : 16.3 mm at 125°, 16.3 mm at 130°, and 15.7 mm at 135°. Therefore, caution is necessary to avoid bone perforation during the lag screw insertion.

For basicervical fractures of the femur, in addition to a sliding hip screw, one screw to control rotation is recommended ^{26).27)}. A 6.5-mm, cannulated cancellous screw is generally used to control rotation durinig the operation. Lag screws with a diameter of about 12 mm are used as sliding hip screws. Thus, the size of both together is about 20 mm, but according to the present study, these may not fit within the FNIS in some patients specially those who have dysplastic hip. The main purpose of the cancellous screw is not to increase postoperative fixation, but rather to control rotation during lag screw insertion. Therefore, in patients in whom the FNIS is expected to be smaller, the use of a smaller, cannulated cancellous screw should be considered.

In conclusion, this is the first study to analyze the medullary morphology of the proximal femur in Japanese women using CT data. The present findings suggest some risk of bone perforation, especially in dysplastic hips, with internal fixation devices that are currently used. The present study findings may be very useful when developing hip prostheses that are more suitable for Asian patients and when developing new lag screws to improve treatment outcomes in proximal femur fracture.

Study	Hip anatomy	Version (degrees)	Neck shaft angle (degrees)	Offset (mm)
Noble	Primary OA	ND	124.7 ± 7.4	43.0 ± 6.8
Argenson	Primary OA	24.7 ± 8.7	129.2 ± 7.8	40.5 ± 0.4
Sariali	Primary OA	21.9 ± 9.4	129.5 ± 5.5	42.2 ± 5.1
Sugano	Normal hip	22.6 ± 10.6	125.8 ± 6.3	ND
Our study	Normal hip	32.1 ± 9.5	129.7 ± 5.4	39.5 ± 4.0
Argenson	Dysplastic hip	31.1 ± 1.8	130.3 ± 1.2	25.7 ± 1.7
Sugano	Dysplastic hip	34.0 ± 16.0	127.9 ± 8.9	ND
Our study	Dysplastic hip	36.4 ± 11.4	132.3 ± 8.9	33.6 ± 4.3

Table 2. Mean values of parameters measured in literature

OA = osteoarthritis; ND = not determined

Table 3. Size of the lag screws sold in Japanese market

Trade name	Company	Diameter (mm)
PFNA	DePuy Synthes	10.3
Gamma nail	Striker	10.5
IMHS	Smith & Nephew	11.0
ITST	Zimmer	11.0
Ω Hip screw	Striker	12.0
DHS	DePuy Synthes	12.5
Inter TAN	Smith & Nephew	15.3

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Conflict of interest statement

The authors have no conflicts of interest to disclose.

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